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NeuroImage xxx (2014) xxx-xxx

# ELSEVIER

Contents lists available at ScienceDirect

## NeuroImage



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YNIMG-11683; No. of pages: 6; 4C: 3, 4

journal homepage: www.elsevier.com/locate/ynimg

## Functional brain networks contributing to the Parieto-Frontal Integration Theory of Intelligence

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6 ARTICLE INFO

Accepted 24 September 2014

Independent component analysis (ICA)

Functional magnetic resonance imaging (fMRI)

Available online xxxx

Article history:

Keywords:

Intelligence

Reasoning

Networks

7

8

9

10

11

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13

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## ABSTRACT

The refinement of localization of intelligence in the human brain is converging onto a distributed network 16 that broadly conforms to the Parieto-Frontal Integration Theory (P-FIT). While this theory has received support 17 in the neuroimaging literature, no functional magnetic resonance imaging study to date has conducted a 18 whole-brain network-wise examination of the changes during engagement in tasks that are reliable measures 19 of general intelligence (e.g., Raven's Progressive Matrices Test; RPM). Seventy-nine healthy subjects were 20 scanned while solving RPM problems and during rest. Functional networks were extracted from the RPM and 21 resting state data using Independent Component Analysis. Twenty-nine networks were identified, 26 of which 22 were detected in both conditions. Fourteen networks were significantly correlated with the RPM task. The 23 networks' spatial maps and functional connectivity measures at 3 frequency levels (low, medium, & high) 24 were compared between the RPM and rest conditions. The regions involved in the networks that were found 25 to be task related were consistent with the P-FIT, localizing to the bilateral medial frontal and parietal regions, 26 right superior frontal lobule, and the right cingulate gyrus. Functional connectivity in multiple component 27 pairs was differentially affected across all frequency levels during the RPM task. Our findings demonstrate that 28 functional brain networks are more stable than previously thought, and maintain their general features across 29 resting state and engagement in a complex cognitive task. The described spatial and functional connectivity 30 alterations that such components undergo during fluid reasoning provide a network-wise framework of the 31 P-FIT that can be valuable for further, network based, neuroimaging inquiries regarding the neural underpinnings 32 of intelligence. 33

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3739 Introduction

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### Modern neuroimaging techniques have allowed for increasingly 40 41 fine-grained inquiries regarding the structural and functional brain correlates of human intelligence. Such techniques have evolved from 42early focus on discrete regional associations (Andreasen et al., 1993) 43to increasingly sophisticated inquiries that regard the brain as a 44 45network (van den Heuvel et al., 2009). While most early studies focused on the frontal lobes as the primary locus of human intelligence (Duncan 46 et al., 2000; Gray et al., 2003), a review of structural and task-related 47 48 functional neuroimaging literature suggested that the integrity of a distributed network involving the parietal and frontal regions best 49accounted for individual differences in intelligence (P-FIT; Jung and 5051Haier, 2007). The theory has been supported by multiple brain lesion 52studies and analyses of healthy controls' cognitive data across different 53neuroimaging modalities (Colom et al., 2009; Deary et al., 2010;

Gläscher et al., 2010; Li et al., 2009; Song et al., 2008). While the P-FIT

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http://dx.doi.org/10.1016/j.neuroimage.2014.09.055 1053-8119/© 2014 Published by Elsevier Inc. has received substantial attention from the intelligence community 55 (Barbey et al., 2012; Deary, 2012; Langer et al., 2012; Luders et al., 56 2009), the broad nature of the theory's scope leaves much ambiguity 57 for further investigations. This study thus aimed to test the P-FIT by 58 isolating the specific functional brain networks that may contribute to 59 it, and examine the changes such networks undergo in terms of their 60 spatial distributions and inter-network connection strengths during a 61 fluid reasoning task. 62

Our understanding of whole-brain processes has progressed sub- 63 stantially since the discovery of inter-hemispheric functional correla- 64 tions in the motor cortex (Biswal et al., 1995). The existence of 65 numerous functional brain networks, or brain regions that exhibit 66 high degrees of intrinsic functional coherence, has since been confirmed 67 using various approaches (Allen et al., 2012b). Analyses of such 68 networks have demonstrated significant relationships between 69 their various properties and cognitive functioning, providing a viable 70 approach for investigating and detecting functional abnormalities in 71 neurological and psychiatric disorders (Garrity et al., 2007; Jafri et al., 72 2008; Vakhtin et al., 2013). The network-wise approach produces read-73 ily interpretable results, and is a useful tool for establishing a framework 74 for better understanding human cognition (Bressler and Menon, 2010). 75

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76 Using independent component analysis (ICA; Bell and Sejnowski, 77 1995), the spatial distributions of resting state functional brain 78 networks have been shown to be stable across multiple independent 79 functional magnetic resonance imaging (fMRI) data sets, with their functions having been inferred using previously established roles of 80 the involved anatomical regions (Allen et al., 2012a, 2012b). The spatial 81 changes that such networks undergo as a response to cognitive engage-82 ment, however, have not been studied extensively. While maintaining 83 84 their general features, multiple ICA-derived networks have previously 85 been shown to alter their spatial distributions during an auditory 86 oddball task (Calhoun et al., 2008). The robustness of such components during engagement in complex tasks, however, is yet to be investigated. 87

The Raven's Progressive Matrices Test (RPM; Raven, 2000) has been 88 89 determined to be one of the best tools for measuring fluid reasoning ability, which in turn is highly related to general intelligence (Snow 90 et al., 1984). The task is based on visual stimuli, overcoming the 91 challenges presented by using verbally mediated tasks to measure 92 intelligence in multicultural samples. Previous neuroimaging studies 93 have revealed that fluid cognitive processes induced by RPM activate 94 areas consistent with the P-FIT, localizing to the bilateral frontal and 95 parietal regions (Duncan et al., 2000; Haier et al., 1988; Kroger et al., 96 97 2002; Prabhakaran et al., 1997). We therefore considered the RPM 98 task as a suitable candidate for inducing activity within the functional 99 brain networks that contribute to general intelligence and comparing them to their resting states. Since the performance on measures that 100 assess fluid reasoning (e.g., Ravens Progressive Matrices) represents 101 relatively complex cognitive processes, we hypothesized that 102103 widespread spatial redistributions of functional networks would be observed during fluid reasoning when compared to during rest. 104 Given the widespread spatial effects that cognitive load is able to 105induce in functional brain networks, we expected parallel changes in 106 107levels of functional network connectivity (FNC) between different pairs of networks. While parieto-frontal connectivity has been asso-108 ciated with higher levels of intelligence in both adults and children 109 (Langeslag et al., 2013; Song et al., 2008), the specific networks 110 involved have not been identified. Importantly, we hypothesized 111 that such changes in FNC between rest and fluid reasoning tasks 112would not be consistent across different frequencies of the networks' 113 time courses. While it has been shown that functional brain 114 networks primarily exhibit low frequency oscillations and tend to 115rely on these frequencies in their connections to each other (Cordes 116 117 et al., 2000), such effects appear to be predominant in sensorimotor, visual, language, and auditory networks. Since such networks are of 118 little interest in our goal of investigating complex cognitive processes 119 involved in fluid reasoning, we hypothesized that FNC in cognitive, 120 default-mode (DMN), and attention networks may not be limited to 121 122these low frequencies during complex cognitive tasks. Functional connectivity changes evoked by fluid reasoning were therefore explored 123across the full spectrum by examining low, medium, and high frequen-124cy bands. The main purpose of the FNC analysis was to isolate the net-125works and frequencies that contribute to the integration of the frontal 126127and parietal regions, which would subsequently be used as stepping 128stones to investigate their relationships with individual differences in fluid reasoning ability. 129

## 130 Methods

Seventy-nine subjects (46 males, 21.7  $\pm$  3.1 years old) were recruit-131 ed for the study from the University of New Mexico (UNM), Albuquer-132que, NM, USA. Prior to study enrollment, each participant signed a 133 consent form explaining the procedures and their potential risks. 134The study and consent form were approved by the UNM Institutional 135Review Board. All subjects were screened for and excluded if they 136reported any past major head injuries, psychiatric or neurological 137 138 disorders, substance abuse, and intake of any psychoactive medications.

The fMRI data were collected using a 3-T Siemens Trio scanner at the 139 Mind Research Network (MRN), Albuquerque, NM. Each participant 140 went through 3 sessions in the scanner: a resting state scan and 2 141 sessions while solving problems from the Standard and Advanced 142 Raven's Progressive Matrices Test (Raven, 1990). Ten matrices were 143 pseudorandomly sampled from six versions of the test, including all 144 difficulty levels of the items, for each RPM session. The RPM sessions 145 consisted of 10 problems each, with each matrix presented at the center 146 of the screen and four possible answer choices below. Subjects made 147 selections by pressing one of four buttons corresponding to the index 148 and middle finger of both hands. Each problem was presented for 149 15 s, with a standard 15-second interstimulus interval maintained 150 throughout each block, during which a cross hair was presented. All 151 participants went through 2 training sessions on the RPM task before 152 their fMRI scans, with none of the problems being presented more 153 than once. During the resting state scan, participants were instructed 154 to stare at a fixation cross presented on the screen in front of them, 155 relax, and think of nothing in particular. 156

The T2\*-weighted functional images were collected using a 157 gradient-echo echo planar imaging sequence with an echo time of 158 29 ms, repetition time of 2 s, flip angle of 75°, slice thickness of 159 3.5 mm, distance factor of 30%, field of view of 240 mm, matrix size 160 of  $64 \times 64$  voxels, and voxel size of  $3.8 \text{ mm} \times 3.8 \text{ mm} \times 3.5 \text{ mm}$ . 161 A total of 5 min, 16 s of resting state data were collected, while 162 each RPM scan lasted 5 min and 50 s. The resulting data were slice 163 timing-corrected and smoothed with a 10 mm kernel using the 164 automated neuroimaging pipeline set up at MRN, which is described 165 in further detail elsewhere (Bockholt et al., 2010; Scott et al., 2011). 166 Data from subjects who moved more than 3.5 mm during any single 167 inter-scan period were excluded from further analyses.

Spatial independent component analysis was used to examine the 169 temporal correlations in signal fluctuations between multiple brain 170 regions, producing a set of independent components with high intrinsic 171 temporal coherences that were maximally independent in space. The 172 algorithm utilizes blind source separation to reduce the data to a 173 number of components specified by the user. Its data-driven nature 174 makes it applicable to resting state scans, which do not possess any tem- 175 poral information necessary for conventional fMRI analyses. We used 176 the Group ICA of fMRI Toolbox (GIFT; http://mialab.mrn.org/software) 177 to separately extract 75 components from the resting state and task 178 sessions, producing a whole-head spatial t-map and a signal time course 179 for each one. Non-artifactual functional brain networks were then se- 180 lected from the resulting data sets according to previously identified 181 components (Allen et al., 2011; Smith et al., 2009), and all further 182 analyses were concerned solely with such networks. Spatial cross- 183 correlations of networks were performed between resting and RPM 184 sessions in order to detect networks present in both conditions, 185 deeming a network stable if its Pearson's r was greater or equal to 0.5. 186

Using the Statistical Parametric Toolbox 8 (SPM8), a unique be- 187 havioral block design was created for each subject and RPM session, 188 modeling the time interval during which the problem was presented 189 on the screen. The model was convolved with the canonical hemody- 190 namic response function, and all the subjects' data were horizontally 191 concatenated within each session. Likewise, each network's time 192 course was horizontally concatenated across subjects in each ses- 193 sion, and the two variables were entered into a regression analysis 194 for all networks in every RPM session. Components were classified 195 as task related if their time courses were significantly correlated with the behavioral model (FDR p = 0.001).

All networks' whole-head spatial maps from each session (rest, 198 RPM1, and RPM2) were z-scaled and entered into a within-subject 199 ANOVA to investigate the effects of RPM task on networks' spatial 200 distributions. A spatial mask was used in the analysis, and was 201 obtained by entering all 3 sessions' data from each network into a 202 1 sample *t* test and applying an FDR-corrected threshold of p = 1e-10 203 to the results. 204

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205 Functional connectivity was examined in all possible pairs of 206 functional networks. Three band-pass filters were first applied to each network's time course, producing low (0.01-0.083 Hz), medium 207 208(0.084-0.166 Hz), and high (0.167-0.25 Hz) frequency datasets. We utilized the Functional Connectivity Toolbox (http://mialab.mrn. 209org/software) to obtain a correlation coefficient for each network 210pair's low, medium, and high frequency connectivity in every session 211 and subject. For every network pair, the correlation coefficients were 212213Fisher z-transformed and entered into a mixed linear model with 214session (rest, RPM1, RPM2) and frequency (low, medium, high) as fixed factors and subjects as random factors. 215

## 216 Results

The subjects averaged accuracy rates of .68  $\pm$  .02 and 0.57  $\pm$  .02 217 on the first and second RPM sessions, respectively. A subsequent paired 218 t test revealed the difference in performance between the RPM sessions 219 to be significant (t (78) = 5.41, p < 0.001). Since the difficulty levels 220of the RPM problem sets were the same, this effect is likely attributable 221to fatigue over successive sessions. Since we were not concerned 222with performance-correlated brain activity in this study, however, 223we did not account for this effect in the subsequent analyses of 224225individual networks.

Twenty-nine functional brain networks were identified in the set 226 of 75 independent components produced by GIFT (Fig. 1), and were 227subsequently classified according to function using previous ICA lit-228erature on the anatomical regions involved. The networks included 229230attentional (A1-A6), cognitive (C1-C6), default-mode (D1-D3), sensorimotor (S1-S6), visual (V1-V6), auditory (AU), and basal 231ganglia (BG). Cross-correlations of the network spatial maps between 232233resting state and RPM sessions revealed that 26 of the networks were 234present during both conditions. One sensorimotor network that was detected during rest was not identified during task performance. 235 Likewise, 2 cognitive networks were active only during the task, but 236 not rest. Ten networks' time courses were significantly correlated 237 with their respective behavioral models and thus classified as 238 task-related (FDR p = 0.001). 239

The analysis of networks' spatial distributions revealed significant 240 effects of task in contrast to resting state in multiple components, both 241 related and unrelated to the RPM task. These spatial effects are present-242 ed in Fig. 1 along with the networks' distributions in each condition. The 243 specific regions involved can be found in the Supplementary material. 244 The functional connectivity analysis revealed significant interactions of 245 session and frequency in 14 task-related network pairs (Fig. 2). The 246 interactions were examined in terms of simple effects of session on 247 functional connectivity within each frequency band. The results indicat-248 ed that increases in FNC during fluid reasoning varied across frequencies 249 in different component pairs (Fig. 3). Additional main effects of session 250 were detected in 5 pairs of networks, 3 of which were positive (Fig. 3). 251 The integration of 2 interconnected network systems appeared to be 252 activated by the RPM task; V2–A1–A3–D1 and V2–C2–A2–V1. 253

## Discussion

This is the first fMRI study to contrast networks' spatial distributions 255 and functional connectivity data collected during resting state and 256 engagement in Raven's Progressive Matrices test, a classic measure 257 of general intelligence. We found a discrete set of networks to be 258 associated with fluid reasoning, which largely overlapped regions 259 first identified in the Parieto-Frontal Integration Theory, including 260 the dorsolateral prefrontal cortex, inferior and superior parietal lobule, 261 anterior cingulate, and regions within the temporal and occipital 262 lobes. One of the main weaknesses of the original theory, that it did 263 not explicitly address the network characteristics of the numerous 264



**Fig. 1.** Twenty-nine networks were identified: 6 attentional (A1–A6), 6 cognitive control (C1–C6), 6 visual (V1–V6), 6 sensorimotor (S1–S6), 3 default-mode (D1–D3), auditory (AU), and the basal ganglia (BG). Twenty-six of the networks were detected in both resting state and Raven's Progressive Matrices Test (RPM) conditions. The networks' spatial distributions during rest and performance of Raven's Progressive Matrices task (RPM) are plotted as 1 sample t test statistics on standard-space Montreal Neurological Institute 152 volumes, with warm colors representing intrinsic network coherence values. The RPM–rest contrasts are presented for each network as well, with warm dool colors marking areas of significant increases and decreases, respectively, in intrinsic network coherences during the RPM task, as revealed by the repeated measures ANOVA (FDR p = 0.001). Networks were functionally classified and ranked according to their degrees of task-relatedness. (\*) denotes networks that were significantly related to the RPM task (FDR p = 0.001).

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**Fig. 2.** Functional network connectivity results. The session  $\times$  frequency interaction (left) was significant in 14 pairs of networks (FDR p = 0.001), which are marked by a white dot. Session effects (middle) were detected in 5 pairs of networks (FDR p = 0.001), with each significant bin in which an interaction was not observed marked by a white dot. Frequency effects (right) were found in 8 pairs (FDR p = 0.001), with the white dots marking those in which the interaction was not significant. (\*) indicates that the network was significantly related to the task.

regions identified, is now addressed using ICA, supporting underlying 265266 network characteristics of brain organization involved in fluid 267reasoning ability. While attention and cognitive networks were 268found to be task related, we also found several sensorimotor, visual, and a DMN to be significantly related to the RPM task. Interestingly, 269all frequency bands (low, medium, and high) were represented in sig-270nificant functional connectivity interactions, with two distinct network 271272systems being activated by the RPM task: visual-attention-DMN and 273visual-cognitive-attention.

Most of the functional networks derived from the resting state 274275data were also present during the RPM task, with 26 networks being detected in both conditions. Such networks exhibited high degrees 276277of spatial correlations between resting state and RPM scans, yet demonstrated significant levels of plasticity in their distributions, as seen in the 278spatial results. These networks are thus able to alter their activity levels 279and spatial distributions, while preserving their general spatial features 280even during complex problem solving. Oddly, one of the networks 281



Fig. 3. Functional network connectivity differences induced by the RPM task. Solid lines represent increases in FNC, while the dashed lines represent FNC decreases as networks switch from resting state to performing the task. The frequencies in which such differences were observed are represented by the colors red (high), blue (medium), and green (low).

observed only during rest was classified as a sensorimotor component. 282 Given component S6's spatial distribution and low relatedness to the 283 task, we speculate that the network may be responsible for sensory 284 processes, explaining the network's activity during the resting state 285 scan, often associated with self-referential thoughts, but not while 286 focusing on the RPM task. 287

The C1 component, on the other hand, was significantly related to 288 the task and detected during the RPM task, but not during rest. Given 289 that the component's main functional regions included the bilateral 290 medial frontal and superior temporal gyri, it appears to be consistent 291 with the frontal and temporal regions proposed by the P-FIT to modu- 292 late performance on intelligence measures. In addition, the superior 293 temporal gyri have been implicated to play a role in integration of pre- 294 vious task actions and outcomes with future decision-making strategies 295 (Paulus et al., 2005). An important limitation to our inferences about 296 the networks that were not detected in both conditions is that their 297 responses to cognitive load in comparison to rest could not be deter- 298 mined. Although the C1 network had the highest degree of task related- 299 ness, we were not able to include it in the spatial or FNC analyses. 300 Further investigations of the C1 network should be undertaken in 301 order to establish the extent to which, if any, its coherence during 302 fluid reasoning may be correlated with other aptitudes. We note 303 that the C3 network was also specific to the RPM condition, but not 304 necessarily of interest to this study due to the fact that it was not 305 significantly related to the task. 306

While the task related networks exhibited the most widespread 307 changes in their spatial distributions during the RPM task, multiple 308 other networks were affected by the RPM task to some degree. In fact, 309 the auditory network was the only one in which no spatial effects 310 were detected. The widespread effects of a complex task like RPM 311 were expected, and the functional classification of ICA-derived 312 networks and their task relatedness measures aided us in focusing 313 on the components relevant to fluid reasoning. 314

The regions involved in the networks that were found to be task related were broadly consistent with the P-FIT. Task related attentional 316 networks localized to the bilateral medial frontal and parietal regions, 317 right superior frontal lobule, and the right cingulate gyrus. Cognitive 318 network C2 involves the right and left lateral frontal regions, which 319 have previously been shown to be involved in decision-making processes (Duncan and Owen, 2000). Two sensorimotor networks were task-212 related, with the left motor strip being the main contributor to the S1 component, likely due to the subjects' use of the right hand when indicating responses to problems. Two visual networks were related to the task, and were localized to the bilateral occipital gyri. Finally, 325 only one DMN was significantly related to the RPM task, spanning the bilateral precuneus. Interestingly, the precuneus has been associated 327

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with visualization and imagination ability (Hassabis et al., 2007), likely 328 329 important to visuo-spatial processing demands of the RPM task.

The functional connectivity analysis between task related networks 330 331 revealed that the components utilize a broad range of frequencies in their integration during cognitive load, with significant positive 332 and negative changes observed in low, medium, and high frequencies. 333 Additionally, the V2 network emerged as a hub between two distinct 334 clusters of networks that exhibited increases in FNC: V2-A1-A3-D1 335 336 and V2-C2-A2-V1. Given that the cognitive frontal network C2 is in the latter cluster, we speculate that it may be the network group 337 338responsible for the decision-making processes during fluid reasoning. 339 Further analyses could investigate the relationship between variables of interest such as IQ and the FNC changes that network pairs undergo 340341 when switching from resting state to fluid reasoning.

There are several weaknesses associated with our approach. First, 342 the use of the RPM could be interpreted to bias the functional networks 343 towards fronto-parietal regions. However, the RPM is considered to 344 be the best measures of fluid reasoning ability in the psychometric 345 literature, and is highly correlated with other measures of intelligence 346 (Raven, 2000), thus making it a good proxy measure of the cognitive 347 construct of interest (i.e., "intelligence"). Our sample consisted of 348 young, healthy, college students who were likely of higher intellectual 349 350 capacity than average. Thus, the generalizability of the current results 351 to populations that are older, include patients with neurological and psychiatric disorders, and who are of average or lower intellec-352tual capacity is unknown. Finally, the use of ICA might be construed 353 as artificially segmenting brain regions into maximally independent 354355networks. Two main assumptions are made with ICA: that the sources are independent and that the distributions are non-356 Gaussian. Either or both of these might be violated with respect to 357 functional brain imaging data. We make note that other techniques 358 359 that do not rely on maximal separation of structural or functional 360 brain regions have found a high correspondence between measures 361 of intelligence and those identified with the P-FIT. Future studies utilizing other measures of "intelligence" (e.g., Wechsler Scales, "g"), 362 more diverse samples (e.g., younger/older, broader IQ range), and 363 other sophisticated analyses (e.g., graph theory) will help to determine 364 365 the veracity of our findings over time.

The findings described in this paper provide a network-wise 366 framework for targeting future neuroimaging analyses focusing on 367 fluid reasoning and general intelligence (i.e., "g"). We have isolated 368 369 the functional brain networks that are related to fluid reasoning, which correspond to the model of intelligence proposed by the 370 P-FIT. The described spatial and FNC contrasts between fluid reasoning 371 and rest provide further insight into the network-wise P-FIT 372373 framework, allowing for targeted examinations of aptitude correlates 374with brain function in future studies.

#### Acknowledgments 375

This research was supported by a grant from the John Templeton 04 Foundation entitled "The Neuroscience of Scientific Creativity." 377

#### **Conflict of interest** 379

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The authors have no conflicts to disclose.

#### Appendix A. Supplementary material 382

Supplementary data to this article can be found online at http://dx. 383 384 doi.org/10.1016/j.neuroimage.2014.09.055.

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